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Highlights

T Wave Alternans

Maxillary Sinus in Patients

Discovering Thoughts, Inventing Future

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Intermittent Preexcitation and Electrotonic Modulation of Repolarization as a Cause of Macroscopic T Wave Alternans

By Riyaz Somani, Jane Caldwell & Adrian Baranchuk

Queen's University, Canada

Abstract - Alterations in ventricular depolarization are recognized to lead to inverted T-waves which manifest once the ventricular activation returns to normal. This phenomenon referred to as 'T-wave memory' or 'electrotonic modulation' may be caused by several clinical conditions producing a shift in ventricular depolarization. Currently, T wave alternans (TWA), either macroscopic or microscopic refers to the beat to beat alteration in the repolarization heterogeneity that repeats with every other beat without changes in the QRS complex. We present the case of a 43-year old man with symptomatic intermittent pre-excitation who underwent 24-hour Holter monitoring revealing TWA secondary to electrotonic modulation. It is assumed that this phenomenon does not carry any prognostic significance.

Keywords : *intermittent preexcitation; electrotonic modulation; cardiac memory; T wave alternans.*

GJMR-D Classification : *NLMC Code: QT 34*



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Intermittent Preexcitation and Electrotonic Modulation of Repolarization as a Cause of Macroscopic T Wave Alternans

Riyaz Somani^α, Jane Caldwell^σ & Adrian Baranchuk^ρ

Abstract - Alterations in ventricular depolarization are recognized to lead to inverted T-waves which manifest once the ventricular activation returns to normal. This phenomenon referred to as 'T-wave memory' or 'electrotonic modulation' may be caused by several clinical conditions producing a shift in ventricular depolarization. Currently, T wave alternans (TWA), either macroscopic or microscopic refers to the beat to beat alteration in the repolarization heterogeneity that repeats with every other beat without changes in the QRS complex. We present the case of a 43-year old man with symptomatic intermittent pre-excitation who underwent 24-hour Holter monitoring revealing TWA secondary to electrotonic modulation. It is assumed that this phenomenon does not carry any prognostic significance.

Keywords : *intermittent preexcitation; electrotonic modulation; cardiac memory; T wave alternans.*

I. INTRODUCTION

Transient changes in the sequence of ventricular depolarization are recognized to give rise to gradual changes in ventricular repolarization which manifests as T-wave inversion. Alterations in ventricular depolarization may be caused by several mechanisms including intermittent ventricular pacing, rate-dependent bundle branch block, tachyarrhythmias with aberrant QRS complexes and ventricular preexcitation. The resultant change in ventricular repolarization remains masked by the secondary T-wave changes induced by the conduction disturbance, and are only unveiled once normal ventricular activation is restored. This phenomenon is referred to as 'T-wave memory' or 'electrotonic modulation'¹.

Reports on T wave alternans (TWA) refer to the beat to beat alternation in the repolarization heterogeneity that repeats with every other beat with the same QRS complex and has recently been linked with an increased vulnerability to ventricular arrhythmias in certain conditions such as myocardial ischemia, Prinzmetal's angina, states of altered autonomic tone, electrolyte abnormalities and in the long QT syndrome². We present the case of intermittent pre-excitation as the cause of TWA secondary to electrotonic modulation.

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II. CASE REPORT

A 43-year old man with symptomatic intermittent preexcitation underwent investigations with 24-hour Holter monitoring. The upper rhythm strip (Figure 1) demonstrates the presence of both preexcited (black arrow) and non-preexcited beats (dotted arrow). In the lower rhythm strip (Figure 1), the corresponding T-wave morphology is seen to alternate with a positive T-wave in the presence of a preexcited beat (grey arrow) and a negative T-wave in the presence of a non-preexcited beat (white arrow). The electrotonic modulation associated with the intermittent preexcitation produced TWA. The patient subsequently underwent an uncomplicated electrophysiology study with successful radiofrequency ablation of a right mid-septal accessory pathway. Figures 2A (pre-ablation) and 2B (post-ablation) show the development of overt T-wave inversion in leads II, III and aVF (post-ablation of the accessory pathway) in association with normalization of the QRS complex as a manifestation of cardiac memory³.

III. DISCUSSION

The cellular and electrophysiological basis that gives rise to the T wave observed on a 12-lead electrocardiogram (ECG) remains controversial⁴. Under normal conditions, the concordant polarity of the T wave and the R wave in the surface ECG indicates that the repolarization sequence proceeds in the opposite direction to that followed by the depolarization process⁵. As the direction of ventricular repolarization depends on the course of ventricular depolarization, any shift of the latter results in an instantaneous modification of the T waves, whose spatial orientation tends to be opposite to that of the abnormal QRS complexes. Alterations in the direction of depolarization, through pre-excitation as highlighted in this case, may give rise to changes in ventricular repolarization that are unmasked once normal ventricular activation is restored.

In the present case, the conditioning stimulus giving rise to the altered depolarization, and subsequent repolarization, was only present in alternating beats which consequently resulted in the generation of TWA. TWA has been reported to be associated with an increased vulnerability to ventricular arrhythmias in a

variety of pathophysiological conditions. In the present case, we demonstrate that TWA may be caused by electrotonic modulation associated with intermittent pre-excitation, although there is no suggestion that in this context the TWA seen is of any prognostic relevance.

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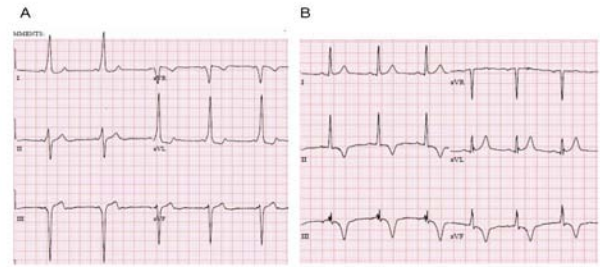


Figure 2

Limb leads pre (A) and post (B) ablation showing the development of overt T-wave inversion in leads II, III and aVF (post-ablation of the accessory pathway) in association with normalization of the QRS complex as a manifestation of cardiac memory.

FIGURE LEGENDS

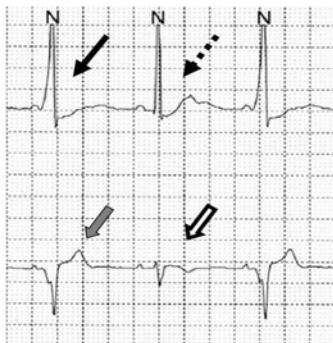


Figure 1

The upper rhythm strip demonstrates the presence of both preexcited (black arrow) and non-preexcited beats (dotted arrow). In the lower rhythm strip the corresponding T-wave morphology is seen to alternate with a positive T-wave in the presence of a preexcited beat (grey arrow) and a negative T-wave in the presence of a non-preexcited beat (white arrow). The electrotonic modulation associated with the intermittent preexcitation produced TWA.



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Characterization of Maxillary Sinus in Patients with Facial Pain using Ultrasound

By Alsaffi Ahmed Abdalla, Shaza Abdelgafoor Abdelgadir,
Caroline Edward Ayad & Amel Gadad

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Abstract- Objectives: This study dealt with characterization of maxillary sinus in patients with facial pain using ultrasound.

Methods: It was carried out on 50 patients complaining of maxillary sinus problems who were referred to the National Center of Ear, Nose and Throat Khartoum-Sudan. The instruments used were; Aloka SSD 500, Honda HS2000 portable with curvilinear probe 3.5MHz, and General Electric LOGIQ5 Mobile with curvilinear and linear probe (3.5MHz, 10MHz).

Results: patients were 27males (54%) and 23 females (46%), their ages ranging between (20-70 years) and the most affected age group was the range (20-30years). All of them were of maxillary pain (100%), 28 patients (56%) of halitosis, 29 (58%) postnasal drip, 30 (60%), stuffy nose, 27 (54%) fever and 17(34%) with of malaise. All patients were diagnosed previously by computerized tomography(CT)coronal scans. Ultrasound findings in the maxillary sinuses of the patients were 30% polyps with hypo echoic cavity, 12% fluid with hypo echoic cavity and the posterior margin was seen, 2% showed cyst with hypo echoic area and well defined borders,12% mucosal thickening, 38% normal sonographic appearance of hyper echoic anterior wall and cavity and the posterior margins were not seen, 6% polyps mucosal thickening with hypo echoic cavity with echogenic bony walls.

Keywords : *ultrasound, pain, maxillary sinuses.*

GJMR-D Classification : *NLMC Code: WN 250*



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Characterization of Maxillary Sinus in Patients with Facial Pain using Ultrasound

Alsaffi Ahmed Abdalla^α, Shaza Abdelgafoor Abdelgadir^σ, Caroline Edward Ayad^ρ & Amel Gadal^ω

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Conclusion: The study concluded that the ultrasound has sensitivity of 76.6% and specificity of 92.2% and ultrasound is beneficial in diagnosis of maxillary sinus pathology and could be used as one of the diagnostic imaging modality ,as it is non invasive ,easy and with no radiation hazards.

Keywords : *ultrasound, pain, maxillary sinuses.*

I. INTRODUCTION

Sinusitis is one of the most common problems affecting the maxillary sinuses. Acute sinusitis may be caused by bacterial infection; Complications of acute bacterial sinusitis (ABRS) may include orbital, intracranial, or soft tissue involvement. Therefore, accurate diagnosis is of major importance and the radiographic imaging is considered as an accurate diagnostic tool.[1]

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The American Academy of Pediatrics Clinical Practice Guideline on the management of sinusitis stated that imaging including radiographs, Computerized Tomography(CT) or magnetic resonance imaging(MRI) ;can serve only as confirmatory measures of sinus disease in patients whose clinical histories are supportive of the diagnosis [2]. The American Academy of Allergy, Asthma and Immunology stated that computed tomography (CT) is the preferred imaging technique for pre-operative evaluation of the paranasal sinuses and that ultrasonography has limited utility, but may be applicable in pregnant women and for determining the amount of retained secretions [3]. Coronal computed tomography (CT) scan of the paranasal sinuses was suggested to be considered in the diagnosis of acute sinusitis [4]. The diagnosis of both acute and chronic sinusitis should be made clinically, and not on the basis of imaging findings alone. CT remains the study of choice for the imaging evaluation of acute and chronic sinusitis, in addition magnetic resonance imaging of the sinuses, orbits, and brain should be performed whenever extensive or multiple complications of sinusitis are suspected. In chronic sinusitis, CT scanning is the "gold standard" for the diagnosis and the management, as well as when surgery is necessary. Nuclear medicine studies and ultrasound are rarely indicated in acute and chronic rhinosinusitis [5]. Diagnostic ultrasound is a non-invasive imaging modality that uses high-frequency sound waves. The great variability of test performance of diagnostic ultrasound in acute sinusitis cites systematic evidence [4]. No risks have been identified with ultrasound evaluation of the paranasal sinuses, but the accuracy of the ultrasound is dependent largely on the examiner's skills.[6]

Therefore this study is to assess the role of ultrasound as another tool in diagnosis of maxillary sinuses in patients with facial pain in order to take part in the detection of maxillary sinuses disorders as well as to characterize normal echo texture of different maxillary sinuses diseases as compared to CT; and to correlate between the ultrasound findings with the patients clinical findings.

II. MATERIAL AND METHODS

The study was conducted at the National Center of Ear, Nose, Throat (ENT) and Head and Neck surgery Khartoum-Sudan, in the period from August to November 2011.

a) Study sample

The sample size consisted of 50 Sudanese patients (females and males) between 20 to 70 years old complaining of maxillary pain, and different clinical symptoms. They were previously diagnosed by CT scan and then were investigated by ultrasonography . Patients whose ages less than 20 years old, and more than 70years old, and patients who have no previous CT scans were excluded. No identification or individual details were published.

b) Instrumentations

Ultrasound machines used were Aloka SSD 500 portable with curvilinear probe 3.5MHz, Honda HS2000 portable with curvilinear probe 3.5MHz and General Electric LOGIQ5 Mobile with curvilinear and linear probes (3.5MHz-10MHz).

c) Method

An approval from the review board and ethics committee of the College of Medical Radiological Science was taken .The patients were examined in sitting position; the U/S gel was applied to the area on the face where the sinuses are located, including the nose, cheekbones and maxillary sinuses. High frequency sound waves produced the image of the internal structures, and a highly ultrasound expertise

Ear, Nose, Throat(ENT) specialist doctor had done the scan and interpreted the data .The patients were scanned by a frequency ranging from 3.5 to 10 MHz. The data were collected using variable patients complaints and they were diagnosed by U/S and the findings were correlated to CT findings.

To find out the accuracy, sensitivity and specificity of ultrasound(U/S) as compared to the Computed Tomography (CT) diagnosis; equations were applied including :A)For U/S accuracy (True positive cases(TP) +True negative cases(TN) /Total number of cases) X 100.B) For U/S Sensitivity(True positive cases(TP) /True positive(TP) +False negative(FN)X100. C) for U/S specificity (True negative cases(TN) /True negative cases(TN) +False positive cases(FP) X100.

III. RESULTS

The following results were for a sample consisted of 50 patients (23 females and 27 males) all were complaining of maxillary pain. The patients were classified according to age. Patients ages ranged from 20-30 years were 21(42%), 31-40years14(28%), 41-50years5(10%), 51-60 3(6%) years, 61-70 7(14%) (Figure1). The following tables showed the results according to the age, gender, complaints and the ultrasound findings.

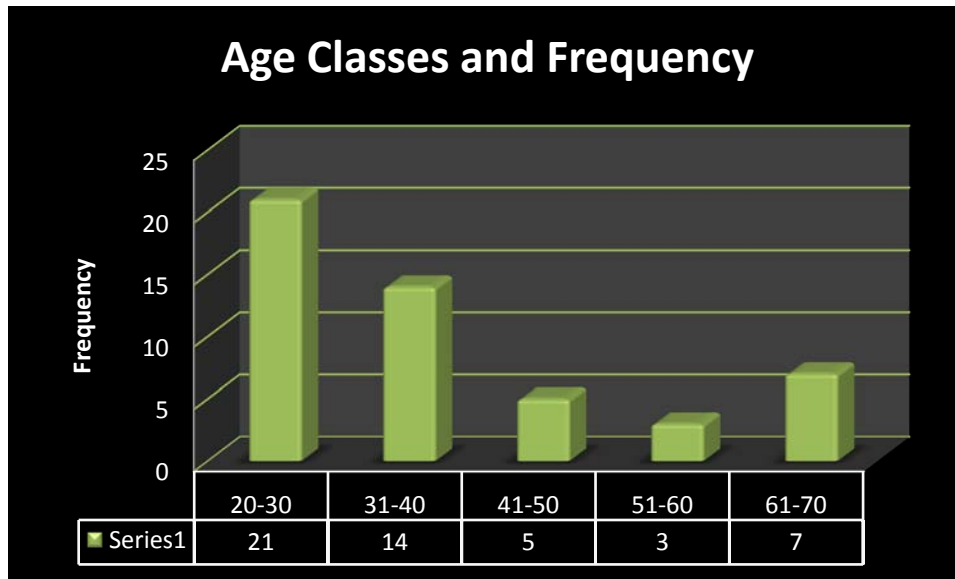


Figure 1 : Age Classes and Frequency

Table 1 : Shows the frequency and percentage of symptoms in the study population

Complains	Number of patients (%)
Fever	27 (54%)
Malaise	17 (34%)
Stuffy nose	30 (60%)
Post nasal drip	29 (58%)
Haltosis	28 (56%)
Pain	50 (100%)

Table 2 : Shows frequency distribution and percentage of ultrasound diagnosis

Ultrasound diagnosis	Frequency (%)
Fluid	6 (12%)
Polyp	15 (30%)
Cyst	1 (2%)
Mucosal Thickening	6 (12%)
Normal	19 (38%)
Polypoidy mucosal thickening	3 (6%)
Total	50 (100%)

Table 3 : Shows the frequency of ultrasound findings according to the patient's gender

Gender	Fluid	Mucosa Thickening	Normal	Polyps	Cyst	Polypoidy mucosal thickening
Male	4	2	12	9	0	0
Female	2	4	7	6	1	3
Total	6	6	19	15	1	3

Table 4 : Comparison of Diagnosis of Maxillary sinuses using Ultrasound and other similar studies

Auther	Ultrasound Sensitivity	Ultrasound Spesifity	Modalities used	Number of Patients
Current Study	76.6%	92.2%	CT and Ultrasound	50
Apostolos H. et al [7]	66.7%	94.9%	CT and Ultrasound	56
Fufezan et al [8]	94.9%	98.4	X-Rays and Ultrasound	67

IV. DISCUSSIONS

In recent decade, the Health Care Guideline (2011) stated that the diagnosis of acute sinusitis should be based on the presenting symptoms, history, and clinical examination. It noted that plain X-rays for sinus and other imaging tests are usually not necessary in making the diagnosis of acute sinusitis due to their poor sensitivity and specificity limits. Other published studies of ultrasound of the paranasal sinuses do not permit assessment of the sensitivity or specificity of the technique compared to the gold standard of CT scanning. [9]

The Agency for Healthcare Research and Quality (AHRQ) evidence report on Acute Bacterial sinusitis does not address ultrasound of the sinuses [10]

This study assessed the ultrasonography as another tool in the diagnosis of maxillary sinuses disorders in patients with pain in order to analyze whether ultrasonography with a reasonable degree of confidence and can replace radiography in the diagnosis of sinusitis. Fifty patients from the national center of ENT diseases and head and neck center who were previously diagnosed by CT, were investigated by ultrasound, the study showed different maxillary sinus ultrasound diagnosis related to age, gender and complaints.

The frequency distribution was according to gender (table 3), there were 27 males (54%) and 23 females (46%) out of total 50 patients (100%) with maxillary sinus pain. These results support the fact that the males were more affected than females.

The study showed the frequency and percentage regarding to age group (Figure1), the most affected age group was the group (20-30) years constituting 42%.

The frequency and percentage of the patient's complaints (table1) revealed that 50/50 (100%) complain of pain followed by stuffy nose 30/50 (60%) as compared to the other complaints.

The frequency distribution and percentage of ultrasound diagnosis (table 2), clarifies that the normal U/S appearance was found in 19/50 constituting 38%, followed by polyps, mucosal thickening and cysts.

Ultrasonography character and findings of the maxillary sinuses were 30% polyps with hypo echoic cavity, 12% fluid with hypo echoic cavity with posterior margin was seen, 2% cyst with hypo echoic area with well defined borders, 12% mucosal thickening, 38% normal sonographic appearance of hyper echoic anterior wall and cavity and the posterior margins were not seen, 6% polypoidy mucosal thickening with hypo echoic cavity and echogenic bony walls.

From the study, the patients suffered from maxillary pain represented (100%), halitosis (56%), stuffy nose (60%), postnasal drip (58%), fever (54%), and malaise (34%).

When comparing the Ultrasound findings with the CT findings; the study showed that the ultrasound has Sensitivity of 76.6% and specificity of 92.2%

Regarding the results and comparing to what was mentioned by (AHRQ); Ultrasound is proposed for demonstrating mucosal wall thickening, focal soft tissue

masses, and complex collections in the paranasal sinuses.

Ultrasound is a painless non-invasive diagnostic procedure and no risks have been identified with ultrasound evaluation of the paranasal sinuses, but the accuracy of the ultrasound is dependent largely on the examiner's skills and to achieve this purpose; this study was done by a highly experience ENT specialist with ultrasonography of excellent performance. The study concluded that paranasal sinus ultrasound has been proposed as best diagnostic imaging modality to confirm the diagnosis of clinical sinuses diseases.

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Development of First Proto-Types of a Low-Cost Computer based Solid-State Spirometer for Application in Rural Health-Care Centres across India

By Paurus Mehta & Vineet Sinha

Bhabha Atomic Research Centre, India

Abstract - India being an emerging economy, it concentrates maximum resources towards indigenization of various technologies making them economically viable to the general population. Presently roughly half of the country dwells in villages and small towns where even basic sanitation and primary health-care facilities are virtually non-existent. Deteriorating environmental conditions have lead to increased susceptibility to various respiratory diseases prompting an early diagnosis from preventive health considerations.

All these factors contribute to a product development philosophy which addresses cost considerations more profoundly in addition to technical accuracy. This paper demonstrates the development of a low cost, portable Spirometer for application in rural health-care centres across India.

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Keywords : *pneumotachograph, fleisch type mouthpiece & full vital capacity.*

GJMR-D Classification : *NLMC Code : W 84.6, WN 17*



Strictly as per the compliance and regulations of:



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1. INTRODUCTION

• Historical Perspective

Indians are genetically at higher risk of developing cardio and pulmonary diseases. Being a developing country, India lacks even basic health-care infrastructure in its far flung rural villages. With the gradual progress in development meaning life-style related diseases like heart-disease, diabetes, renal diseases etc. have taken a toll on the population. Compounding the problems of wide-spread poverty with

an increase in life-style related diseases necessitates a greater budgetary allocation needed for providing primary health-care. On an average 30% of Indians suffer from various cardio-vascular & pulmonary diseases. Latest statistics reveal that roughly 27 % of India's population falls under the below poverty line category. With the slow pace of economic growth seen in recent years India has not been able to fund rural health-care and poverty alleviation schemes with generous budgets.

• Objectives

Our research is directed towards bridging the cost divide in providing much needed basic health-care for our less-fortunate countrymen living in rural India. As a precursor to providing diagnostic indicators for various diseases, a Spirometer forms an integral piece of equipment to be installed in village health-care centres across India.

• Comparative Statement

Commercially available Spirometers are expensive to be procured for every village clinic considering there are 5,93,731 villages across the Indian sub-continent. An indigenous initiative to develop diagnostic equipment will go a long way in providing sustained supply of health-care equipment for the country.

• Concept and Realization

Spirometry is the technique of measuring the respiratory function of humans. It is most commonly referred to as pulmonary function tests (PFTs) in diagnostic parlance. PFTs employed for measuring lung function parameters like total lung volume, air flow rate and velocity during the inhalation / exhalation cycles give an indicator of lung muscle integrity. These vital parameters are crucial in diagnosing respiratory diseases like asthma, pulmonary fibrosis, cystic fibrosis, and COPD. The outputs of spirometry are generally referred to as pneumotachographs which contain graphical illustrations of Flow-rate versus Volume, Volume versus time & Flow-rate versus time. Commercially available spirometers in the market are often exorbitantly expensive and not within the reach of

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allow these physicians to make more quantitative assessments of their patients' pulmonary health. A training program that would instruct and motivate patients through the Spirometric tests would further

augment the accuracy of clinical diagnosis. Figure 1 example of a test spirogram. The various lung diseases vis-à-vis the indicative figures of Spirometry parameters are enlisted in Table-1.

Table 1 : Tabular form of various diseases versus the indicative (qualitative) figures of Spirometry Parameters

Sr. No.	Diagnosis	Forced Expiration Volume for one second FEV1 (Litres)	Forced Vital Capacity FVC (Litres)	FEV1/FVC
1	Normal Person	Normal	Normal	Normal
2	Airway Obstruction	Low	Normal / Low	Low
3	Airway Restriction	Normal	Low	Low
4	Combination of Obstruction / Restriction	Low	Low	Low

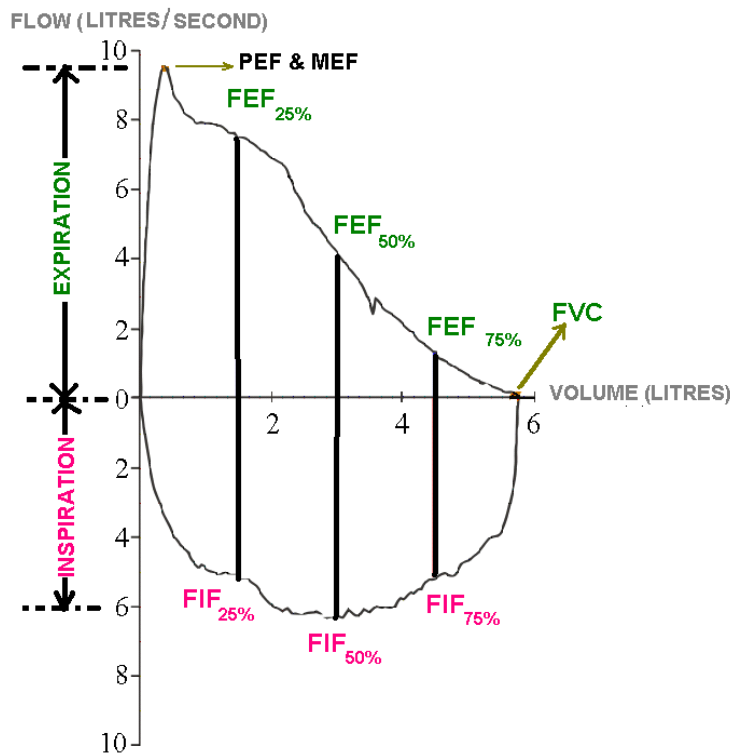


Figure 1 : Graphical illustration of a sample Spirogram

SDI Diagnostic, MicroDirect, and Welch Allyn are among some of the commercial manufacturers of spirometers. SDI Diagnostic manufactures six different spirometers ranging from \$995 to \$2395. The Spirolab II is a top of the line spirometer with salient features touch screen, Bluetooth, and a bidirectional turbine with a price tag of \$2395. Among the commercial brands MicroDirect spirometers are comparatively affordable with a price of \$1419.55. Summarily, nearly all spirometers in the market are far too expensive for use in developing countries.

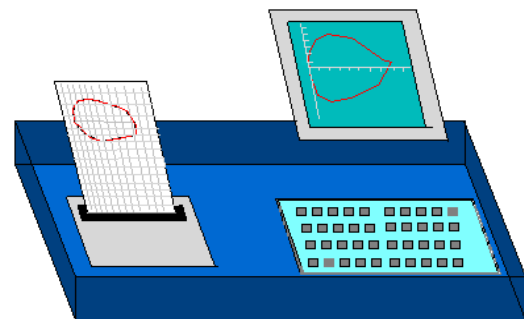


Figure 2 : Illustration of a commercially available Spirometer

There are various approaches to designing Spirometers viz. solid-state pressure sensor approach, volume based sensor approach, Convective heat

transfer, turbine based anemometer design & Air flow acoustics approach. The solid-state pressure sensor approach will be discussed extensively in the later sections. Volume based spirometers work on the principle of measurement of air volume through downward displacement of water. The merits of this approach are its simple design, low cost & a permanent mouth-piece design. The permanent mouthpiece also eliminates the need for a reliable supply of mouthpieces to use the device. This design would also be relatively simple to construct, and repairs would be very basic.

However, this device is quite large in size in comparison to the other designs. The chamber would have to expand to a volume of at least eight liters according to these design constraints, and the elongated tube would also add to the bulk of the device. Reliability is also an issue with this design as the tube contains a significant amount of dead space. This dead space not only weakens the signal, but could also increase the need for calibration.

Hot-wire based spirometers are based on the principle of Convective heat transfer. The rate of cooling is proportional to the rate of flow of fluid through the hot-wire sensor [10]. The value of h depends on the fluid mass flux (density * velocity) and dimension of sensor. The function between h and velocity can be experimentally determined by best fitting the parameters in modified King's law for free convection heat transfer at low Reynolds number (R_e) in a long cylindrical structure.

$$\text{Resistance of hot-wire sensor: } R_s = Ae^{\frac{B}{T_s}} \quad (1)$$

$$\text{Power Delivered to Sensor: } P = hS(T_s - T_f) \quad (2)$$

Where:

- B = a material dependent constant;
- T_s = temperature of the sensor in K;
- R = resistance at temperature T_s
- T_o = reference temperature in K
- R = resistance at temperature T_o
- T_f = Fluid temperature
- h = heat transfer coefficient referred to the sensor surface in W/m^2K
- S = surface area of the sensor.

$$h = C_o + C_1 v^n \quad (3)$$

The hot-wire sensor (Japanese CHEST M.I. INC., Hi- 501) is placed on one arm of Whetstone bridge and excited with constant voltage without negative feedback. The output signal is amplified and digitized by ADC of Lab-VIEW system or prototype system.

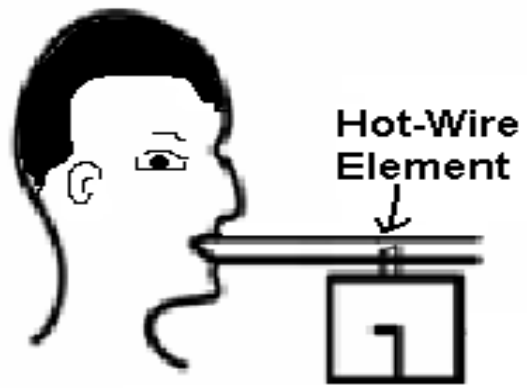


Figure 3 : Illustration of hot-wire based Spirometry technique

The air turbine based spirometers are based on the principle of direct proportionality of rotation speed on flow rate. Some of the demerits of this approach are friction related drag leading to inaccurate results at the fag ends of the respiratory cycle. Hence this leads to a non-linearity of rotation speed at the beginning and end of the breathing cycle.

II. DESIGN OF PRESSURE SENSOR BASED SPIROMETER SYSTEM

a) Principles of Fluid Dynamics

Total Pressure of a fluid flowing through a tube is the sum of the static and dynamic components. Static component of pressure is essentially the pressure exerted on the walls of the tube when the fluid is at rest (velocity = 0 m/s) whereas the dynamic component gives the pressure exerted by fluid when in motion. The dynamic pressure is dimensionally referred to as the change in kinetic energy per unit volume. Our spirometer system is designed to work on the principle of measurement of dynamic pressure of a fluid when it traverses a tube.

$$\text{Dynamic Pressure: } P = \frac{1}{2} \rho v^2 \quad (4)$$

Where: ρ = Density of Air at 300° K
 v = Velocity of flow of fluid

Once the dynamic pressure is extracted from the sensor, the Velocity of flow can be determined using equation 4.

$$\text{Flow-rate: } F = A \times \text{Velocity} \quad (5)$$

Where: A = Area of cross-section of tube

Total Volume of air can be determined by equation 6.

$$\text{Volume of Air: } V = \int_{t1}^{t2} F \cdot dt \quad (6)$$



The illustration in figure 4 shows the functional block diagram of the devised spirometer system. The first block is concentrated on the front-end of the system, in this case, the mouthpiece device. The second block is dedicated to the sensing device, in this case a FREESCALE Semiconductors Inc. dual port, MEMS

based pressure sensor (MPXV2010DP). The third level is reserved for the analog signal conditioning function. The fourth and fifth modules contribute towards signal digitization and ultimate display of the output of the system.

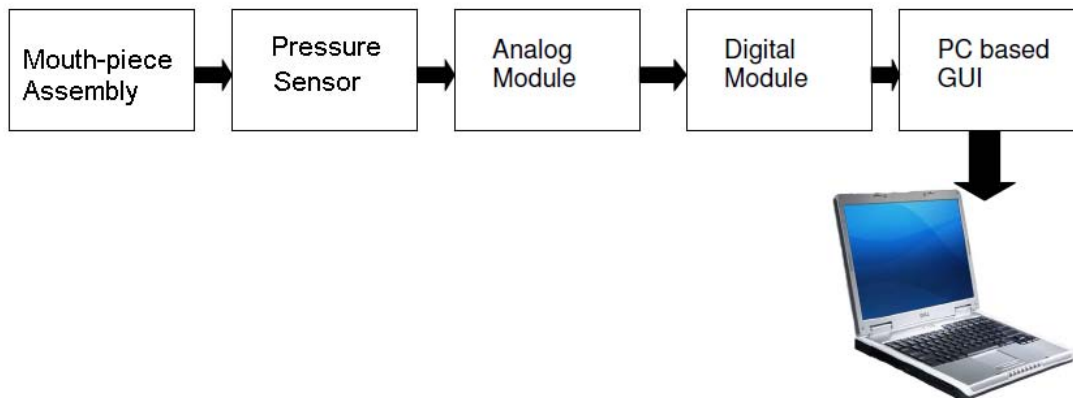


Figure 4 : Functional block diagram of the complete Spirometry System

b) Sensor Calibration

Prior to making any measurement, the pressure sensor needs to be calibrated for its performance. A FLUKE Inc. blood pressure simulator (BP-PUMP2) has been employed for applying a fixed quantum of static pressure on the sensor ports. The positive side port was calibrated first by connecting to the simulator. The applied pressure was varied from 6.7 kPa to 13.3 kPa and the voltage at the output of the analog circuit (described in section II c) was measured. This output voltage was normalized by subtracting the mid-point

potential of 5V (Maximum input swing for ADC) with the output value. This results in a range of voltage values from 0 to 5 V with 2.5V as centre value. The pressure to voltage conversion factor (+ve & -ve ports) was also calculated from the formula given in Table-2. This factor was crucial in deducing the pressure value from the output of the ADC. Alternately, the applied pressure was calibrated using a sphygmomanometer in parallel with the fluke BP simulator and the deviation of pressure values was found to be 1.55% between the mercury readings and our system.

Table 2 : Calibration values for positive side port of sensor

Sr. No.	Pressure (applied) (kPa)	Output Voltage "V _P " (+ve Port) (Volts)	Normalized Voltage (V _P -2.5) (+ve Port) (Volts)	Pressure to Voltage conversion factor [Pressure / (V _P -2.5)] (kPa / Volts)	Average Conversion factor (kPa / Volts)
1	6.7	3.28	0.78	8.58974	8.3907
2	8	3.41	0.91	8.79121	
3	9.3	3.64	1.14	8.15789	
4	10.6	3.79	1.29	8.21705	
5	12	3.95	1.45	8.27586	
6	13.3	4.1	1.6	8.3125	

Table 3 : Calibration values for negative side port of sensor

Sr. No.	Pressure (applied) (kPa)	Output Voltage "V _N " (-ve Port) (Volts)	Normalized Voltage (2.5-V _N) (-ve Port) (Volts)	Pressure to Voltage conversion factor [Pressure / (2.5-V _N)] (kPa / Volts)	Average Conversion factor (kPa / Volts)
1	6.7	1.83	0.67	10.00	9.75734
2	8	1.68	0.82	9.7561	
3	9.3	1.54	0.96	9.6875	
4	10.6	1.40	1.1	9.63636	
5	12	1.27	1.23	9.7561	
6	13.3	1.13	1.37	9.70803	

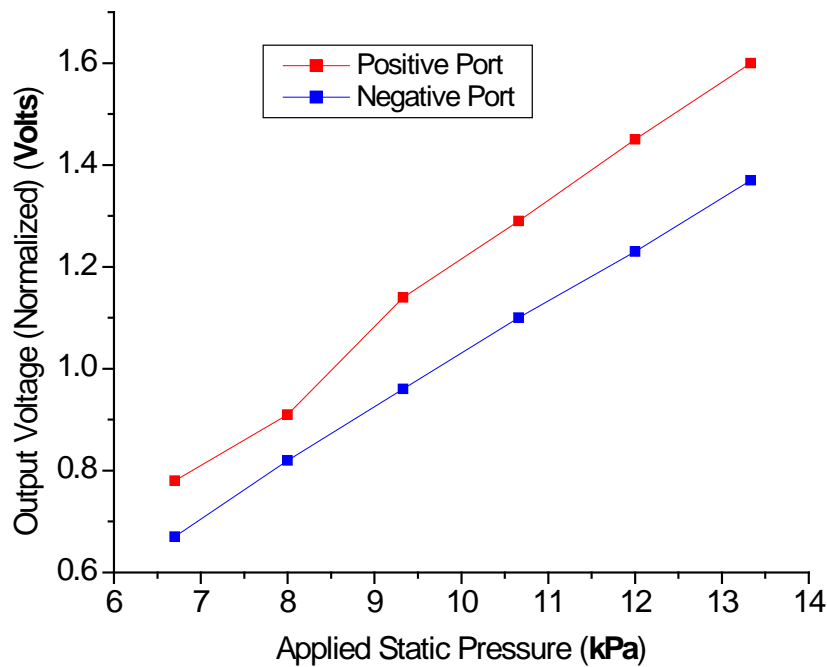


Fig. 5 : Normalized output voltage versus applied static pressure

c) Analog signal conditioning module

The analog circuit (Fig. 6-a) for the Spirometry system consists of instrumentation amplifier (AD624) in conjunction with an OPAMP. The output of the IA is then coupled as input to a general purpose OPAMP (AD713) for further amplification to give a signal large enough to drive the input to an ADC in the digital micro-controller module. Presently, the total gain of the system is 55. Gain can be tuned depending on the value of the output signal from the pressure sensor and the ADC input range. Additionally, level-shifting block is added at the output to prevent the negative drift of output voltage from the negative pressure port of the sensor. This level

shifter is designed with a single low power, low leakage current Quad OPAMP (LMC 6044) in a summation configuration. The input reference voltage is fixed at the mid-gap of the ADC range of 5V. The reference voltage of 2.5V is supplied by a potential divider arrangement consisting of two 1MΩ resistors. The mid-point of the divider is connected to a buffer for voltage stability and the output of the buffer is connected to the non-inverting terminal of the level shifter OPAMP. A photographic illustration of the realization of the analog circuit over multipurpose PCB is shown in figure 6-b.

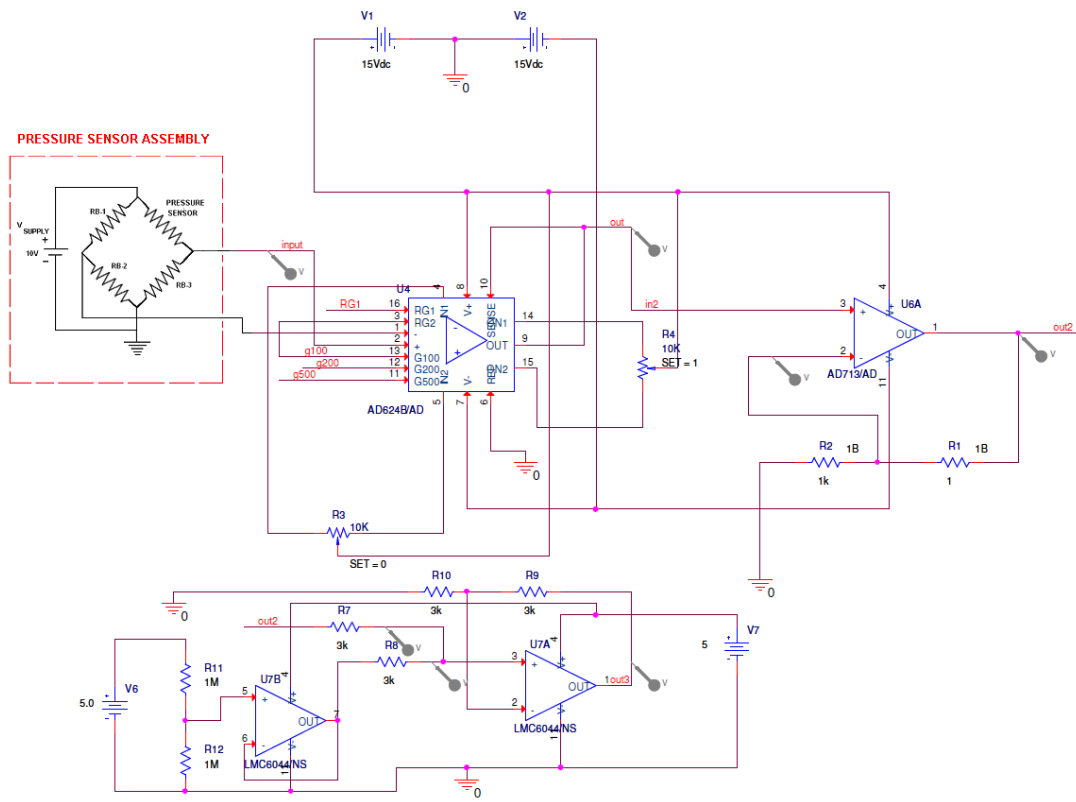


Fig. 6 (a) : Schematic diagram of the Analog signal conditional module

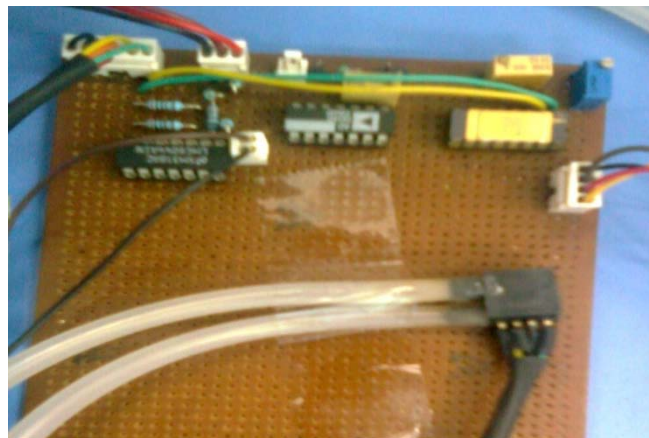


Fig. 6 (b) : Photograph of the realization of the analog circuit over multipurpose PCB

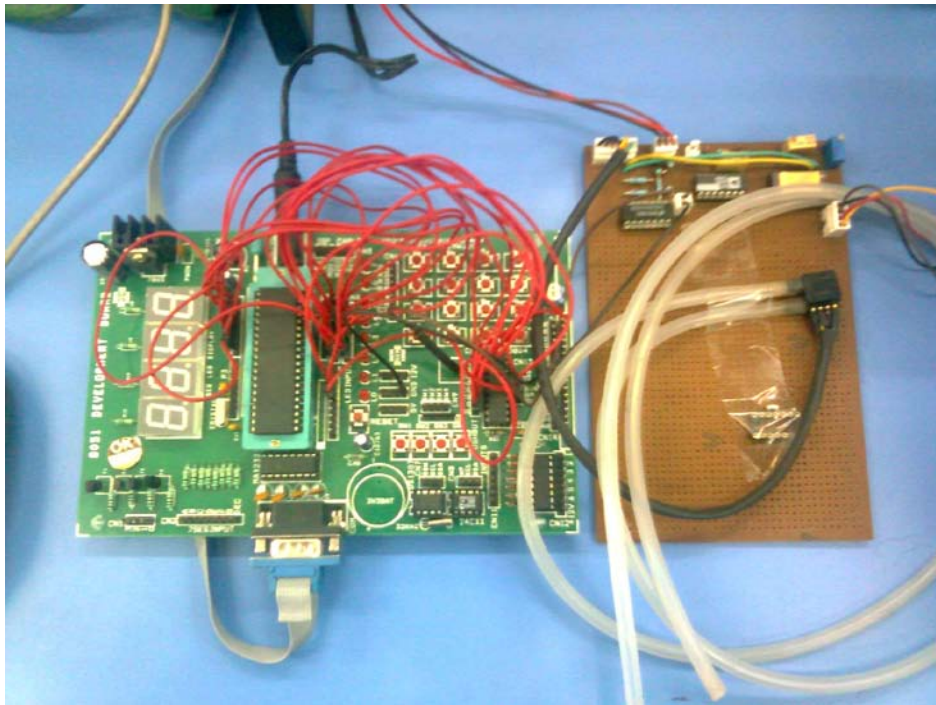


Figure 6 (c) : Photograph of the complete analog & digital setup

d) *Design of micro-controller firmware*

A digital module (Fig. 6-c) consisting of the analog to digital converter (ADC0804), RS-232 interface & microcontroller (89V51RD2) was employed to convert the analog signal to a digital output and send data in digital form to the computer via the RS-232 port. The sampling frequency of the ADC was set at 700 Hz for digitizing the input signal. Since the input signal is of very low frequency (<10Hz), a sampling frequency of 700Hz is enough to give good real time performance. The flow of the implemented micro-controller firmware program has been illustrated in figure 7. To begin with, the read, write & interrupt pins of the ADC were assigned to P2⁵ (Pin-5 of Port-2), P2⁶ & P2⁷ of the micro-controller. The next step was to initialize the counter and assign pin-0 of Port 3 to a variable called LED which would then be called after conversion is performed. The next block of the flow chart is dedicated for setting the buffer for transferring data to serial port. Then comes the block for setting parameters for beginning the conversion cycle for the ADC to Read/Write and transmit. The subsequent block for setting the timer interrupt for a sampling frequency of 700 Hz, calling the ADC from the timer interrupt ensuring a timer synchronized conversion & setting the output to toggle the port assigned to variable LED. The subsequent blocks are dedicated to setting the timer 1 in mode 2 for a baud rate of 9600 bps, enabling interrupt and starting timer.

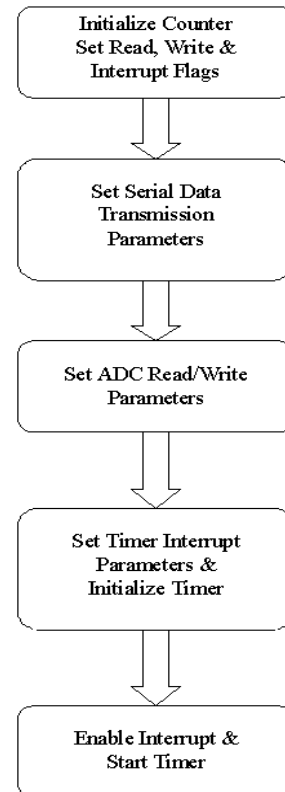


Figure 7: Flow chart of the implemented micro-controller program

e) *Design of Computer Software*

The digital module sends data to the computer, which then had to be interpreted and plotted. For this purpose an interface program has been coded using the Lab-Windows software. Some of the salient features of the developed GUI software are as follows:

- Real-time acquisition and display of data
- Facility to print output panel in PDF format
- Ability to save plotted data in raw ASCII format
- Facility to enter patient name in panel
- Control of acquisition and display by use of Stop and Resume buttons
- Display of raw ADC data in Decimal format
- Display of ADC input voltage in real time graph & mean voltage in numeric format.
- Display of mean values of Pressure, Flow-rate (m^3/s & Litre/s), Volume, Full Vital Capacity (FVC), Forced Expiration Flow (FEF 100%), & Forced Expiration Volume (FEV).
- Real-time graphical output of Pressure v/s time, Flow-rate (Litre/s) v/s time, Flow-rate v/s Volume (Spirograph).

The spirometer system including the software has been tested with an indigenously designed prototype mouthpiece. The system has been tested on a real human subject and results are discussed in the following section. Figure 8 shows a snapshot of the function panel of the designed software. The spirograph shows a value of volume, which is having a zero error of 2 litres, which meant that the actual total volume of air inhaled/exhaled is roughly 6 litres. The software also allows for entering calibrated zero-error values of pressure and voltage making it highly versatile. It also features a real-time display of digitized voltage for cross-checking of output data.

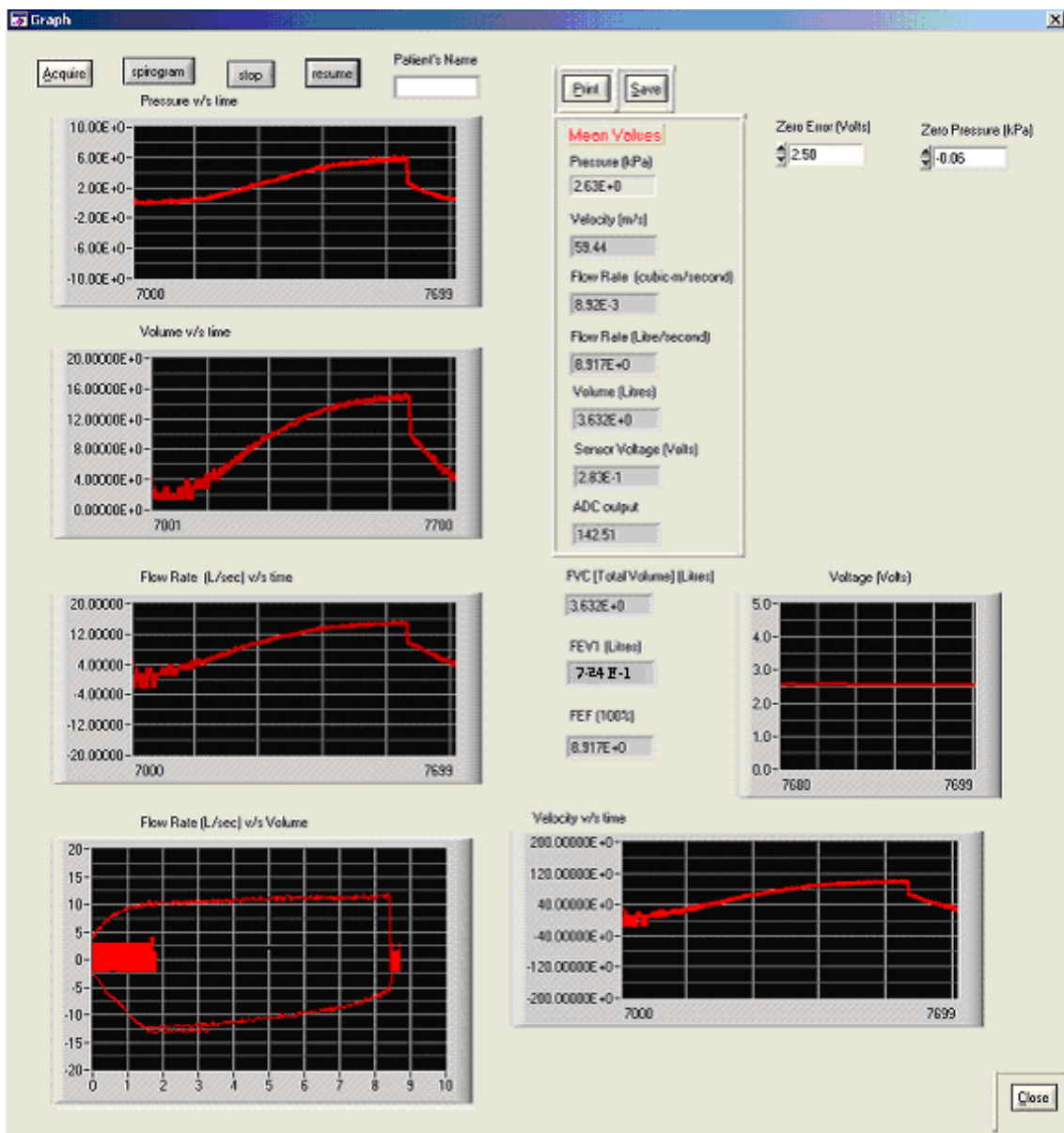


Figure 8 : Snapshot of the GUI program for the Spirometer System showing a sample Spirograph taken for a human subject

f) Design of Mouthpiece

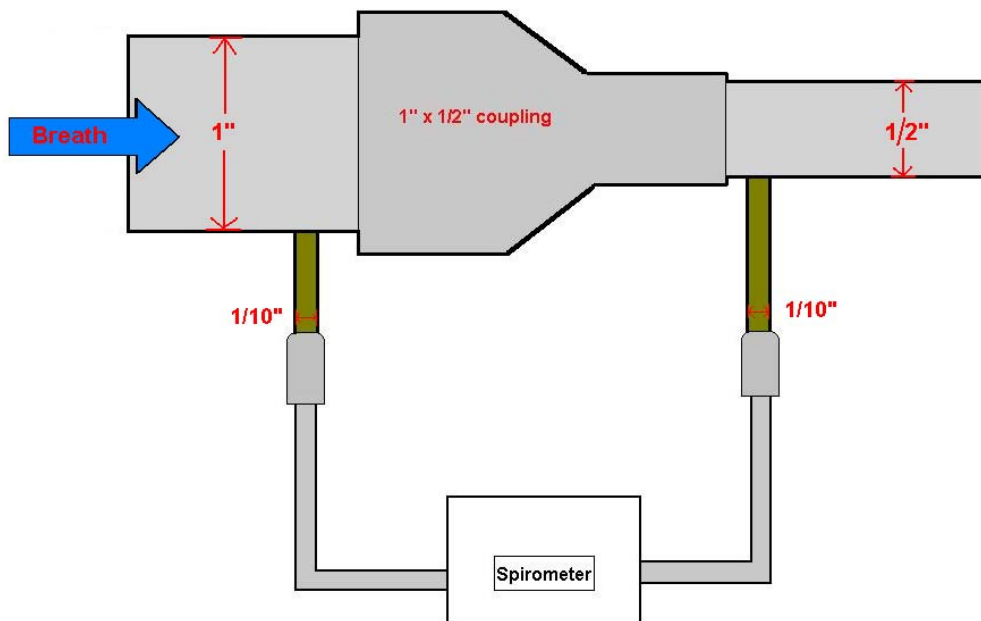


Figure 9 (a) : Illustration depicting the designed mouthpiece with dimensions

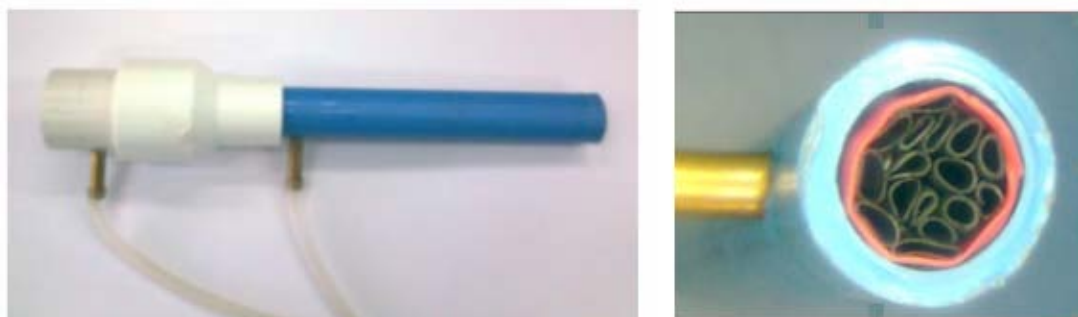


Figure 9 (b) : Photograph of the fabricated mouthpiece (left) and cross-section showing the laminar flow resistor (right)

The first proto-type of the spirometer mouthpiece has been designed and fabricated using in-house facilities. The mouthpiece has been designed for a 50% drop in pressure across its length. The design essentially consists of two PVC pipes connected via a coupling. The tube facing the patient was of 1 inch diameter which was connected to a 1" to 0.5" reduction coupling. The latter end of this coupling was connected to a 0.5" PVC pipe. The pressure sensing ports connecting the pressure sensor with the mouthpiece were fixed at either ends of the coupling assembly in a linear and coplanar fashion. There is a Fleisch type air resistance assembly that converts the turbulent flow input from the patient to laminar flow for better sensing accuracy (figure 9-b) and it is placed in the space between the sensing ports. The patient blows air from the left end (Fig. 9-a) resulting in a pressure difference between the ports which is in-turn sensed by the silicon pressure sensor and converted to meaningful output by the system.

III. RESULTS & DISCUSSIONS

The completely developed spirometer assembly together with mouthpiece, analog & digital modules, and software was tested with a human subject. The subject was instructed to follow the standard breathing maneuvers and the data was acquired for real-time calculation of spirometry parameters. The zero-error/tolerance values for various parameters are listed in table 4 below. The area of cross-section of the mouthpiece was $1.5 \times 10^{-4} \text{ m}^2$. Mean values of air velocity, flow-rate & total volume were extracted for each respiratory cycle and tabulated in table 5. The measured volume was correlated with a standard calibration syringe. As seen from figure 10, the air velocity has a direct proportionality w.r.t the flow-rate. A respiratory cycle is such that the velocity and flow-rate are continuously varying functions of time. A time integration of the flow-rate will yield the cumulative volume in one respiratory cycle. The plot in figure 11

exhibits a near linear dependence of the displaced air volume on the flow-rate thereby confirming that the data is taken from a single person, as over a short duration of time, the physical status of the individual remains practically constant.

Table 4 : Tolerance values of various parameters

Parameter	Value
Pressure	0.06 kPa
Volume	0.8 Litres
Velocity	1 m/s
Flow-rate	0.15 L/s

Table 5 : Spirometric Test Results (mean values)

Sr. No.	Velocity m/s	Flow-rate Litre/s	Volume Litres
1	44	6.6	3.13
2	53.9	8.08	3.97
3	65.07	9.75	4.74
4	67.1	10.15	5.04
5	75.18	11.38	5.49
6	82.3	12.35	6.23
7	86.09	12.91	6.48

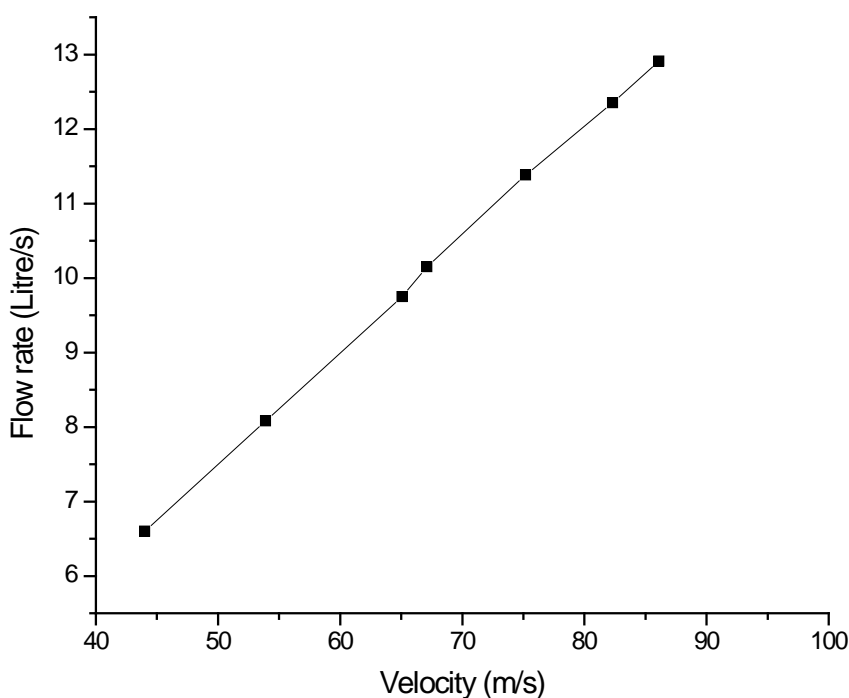


Figure 10 : Plot showing the Velocity versus Flow-rate proportionality



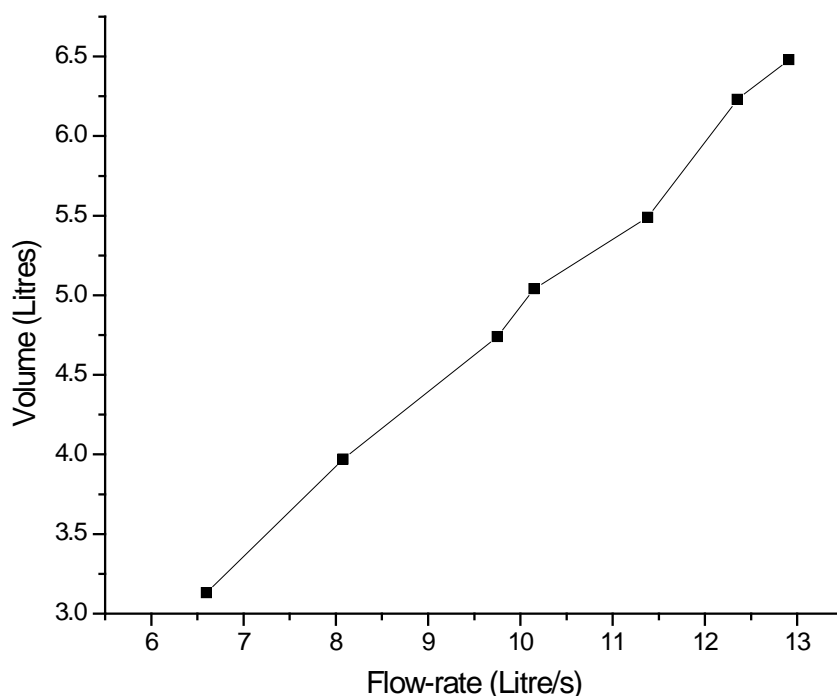


Figure 11: Plot depicting Volume versus Flow-rate for a human subject over various respiratory cycles

IV. CONCLUSIONS

The solid-state sensor approach to realizing a spirometer system has been employed with good degree of success. The pressure sensor has been extensively characterized with calibrated amounts of static pressure and the pressure to voltage conversion factor has been empirically estimated. The analog circuit has been designed with great care to prevent any non-linearity in operation. Micro-controller firmware program has been designed with a view to minimize conversion losses and give real-time data at the output. The computer software has been developed with a view to display significant Spirometric data in real-time. This software has also been designed with a user-friendly approach in mind and gives a fair deal of control to the operator. An indigenous design of a proto-type mouthpiece has been able to achieve good results. Preliminary test results have indicated that the system has performed with a great degree of accuracy. Hence, the first principle's approach to realizing of a Spirometer using a solid-state pressure sensor has succeeded. Extensive trials need to be performed on human subjects to gather statistical data for further analysis.

V. ACKNOWLEDGMENTS

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Establishment of Local Reference of Spleen Length in Sudanese Normal School age Children Sonographically

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Abstract- Objectives: The objectives of this study were to establish a local ultrasonic splenic length which can be used as reference for Sudanese healthy school age children and to determine the normal standards spleen length related to gender, age, body weight, height, body mass index (BMI), and abdominal circumference.

Methods: 215 healthy school-aged children (7–13 years) from city centers were evaluated. Gender, age, weight, height, BMI, and abdominal circumference were determined for each case. The sonographic examination for spleen length was performed with a high resolution real time scanner (SSD-500 Aloka Medical System) fitted with a 3.5MHz convex transducer; all of the measured spleens had a normal position, shape, and echo texture. The children were classified into 7 groups according to age and gender.

Results: The mean length of the spleen was found to be 9.5-10.4cm. There was significant difference between the spleen length in males and females (P -value 0.000), the mean length of spleen in females is greater than in males. A significant relation was found between spleen length and age, weight, height, abdomen circumference and BMI.

GJMR-D Classification : NLMC Code: WN 208



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Conclusion: The spleen length obtained in this study was in different range of values reported in previous studies and a local reference of spleen length was established. We hope that this study contributes to daily clinical practice in ultrasound clinics for interpretation of sonographic examinations for Sudanese school age children regarding the spleen length.

I. INTRODUCTION

The spleen is the largest organ in the reticulo endothelial system. Spleen size can be used as an indicator of disease activity in a variety of disorders of the reticulo endothelial system. [1]

The spleen responds to different pathologic states by dimensional changes. Malaria and sickle cell disease with a geographical bias are known to cause changes in spleen size. A rapid increase in spleen size, secondary to sequestration of red blood cells, platelets and other haematological elements, was observed in

neonates on extracorporeal membrane oxygenation [2, 3, 4]

There are several studies about normal internal organs character [5, 6] All of these are from the populations of Caucasoid and from the populations of Asian, Japan, China, Korea, and India. In the past, Thailand normally used references from American or European references. The problem is that the differences of these factors make the indicators different: race, body structure, genetic, environment, living condition, life style, and food. [7, 8].

Spleen size varies widely according to age also many diseases can affect its size, including infections and malignancy. [9,10]

The variations in the anthropometric features of various populations, races and regions are an established fact. The climate of the zone and the socio-economic status of Sudan, make the population of this region special. There is no comprehensive anthropometric study on the normal measurements of spleen by ultrasonography in Sudanese, and therefore, it was thought to be important to undertake the present study to evaluate the normal measurements of spleen in the school age Sudanese population.

Radiography and radionuclide studies expose the patient to X and gamma radiation [10,11,12,13]. Ultrasonography is the method of choice for the diagnosis of the abdominal pathologies [14]. Sonography is routinely used to determine the internal structures of the body because the examination is real time, three-dimensional and independent of organ function. Ultrasonography is a non-invasive, established, safe, quick and accurate method for the measurement of spleen size. [13]

In Sudan, There is absence of domestic reference for spleen length; and as far as we know, no study was published in the open literature, regarding the spleen length for school age children therefore, the importance of this study lies in finding the normal length of spleen and to determine its correlation with gender, age, height, weight, body mass index (BMI) and abdominal circumference.

II. MATERIALS AND METHODS

The study was done in Alsidigah School and Hamza Ebn Abdmutalib School in Bhari city from January 2012-February 2012.



a) *Ultrasound Machine*

The sonographic examination performed with a high resolution real time scanner (SSD-500 Aloka Medical System Co, Ltd, Tokyo, Japan) with a 3.5MHz convex transducer.

b) *Sample*

A total of 215 (104 males, 111 females) healthy Sudanese children with normal spleen position, shape and echo texture. Any abnormal spleen position, shape and echo texture, children affected with malaria,

malignant spleen diseases, benign spleen conditions, traumatic spleen were excluded.

c) *Measurement Technique for spleen*

Spleen Length was taken by measuring the longest dimension in coronal plane. Longitudinal dimensions in the coronal plane were obtained with the subject in supine or slightly right lateral decubitus position; longitudinal size measurement was performed between the most supero medial and the most infero lateral points of the spleen.

III. RESULTS

Table 1 : Spleen length measurement classes, frequency and percentage

Spleen	Frequency	Percentage
6.5-7.4	28	13.0%
7.5-8.4	43	20.0%
8.5-9.4	56	26.0%
9.5-10.4	67	31.2%
≥ 10.5	21	9.8%
Total	215	100.0%

Table 2 : Descriptive statistics for subject's physical data and spleen length measurement

	BMI	Weight (Kg)	Abdominal circumference	Height (M)	Spleen (cm)
Mean	16.8	32.5	58.2	137.9	9.0
Std. Deviation	±3.4	±10.1	±7.1	±11.0	±1.2
Minimum	10.4	16.0	43.0	112.0	6.7
Maximum	33.6	71.0	83.0	167.0	11.7

Table 3 : mean values of the variables according to age

Variable	Age							Total	P-Value
	7	8	9	10	11	12	13		
BMI	14.4 ± 2.0	14.7 ± 2.2	18.0 ± 4.5	17.0 ± 2.8	16.7 ± 2.7	18.1 ± 2.9	18.9 ± 3.6	16.8 ± 3.4	0.000*
Weight	22.9 ± 3.6	24.1 ± 4.8	32.9 ± 9.3	33.1 ± 7.5	33.5 ± 6.0	38.8 ± 7.7	44.5 ± 10.2	32.5 ± 10.1	0.000*
Abdominal circumference	53.9 ± 4.1	53.5 ± 5.2	60.2 ± 8.5	59.3 ± 6.4	58.8 ± 5.3	59.1 ± 6.8	63.8 ± 7.1	58.2 ± 7.1	0.000*
Height	126.1 ± 5.5	127.6 ± 5.4	134.7 ± 4.3	139.0 ± 7.4	141.4 ± 5.1	146.0 ± 6.5	152.8 ± 8.9	137.9 ± 11.0	0.000*
Spleen	7.9 ± 0.7	7.7 ± 0.6	8.9 ± 1.3	9.3 ± 0.8	9.4 ± 0.6	9.9 ± 0.7	10.1 ± 0.7	9.0 ± 1.2	0.000*

Table 4 : mean values of the variables according to gender

Variable	Gender		Total	P-Value
	Male	Female		
BMI	16.6 ± 2.3	16.9 ± 4.2	16.8 ± 3.4	0.580
Weight	31.6 ± 7.8	33.4 ± 11.8	32.5 ± 10.1	0.195
Abdominal circumference	57.2 ± 5.6	59.3 ± 8.1	58.2 ± 7.1	0.029*
Height	136.9 ± 10.5	138.8 ± 11.4	137.9 ± 11.0	0.203
Spleen	8.7 ± 1.1	9.3 ± 1.1	9.0 ± 1.2	0.000*

From above table we have significant difference between males and females in (Spleen and Abdomen circumference) P-value was less than 0.05, that means the mean length of Spleen and Abdomen circumference in females was more than mean length of Spleen & Abdominal circumference in males, respectively.

Table 5 : mean values of the variables according to age & gender

Age	Gender	BMI*	Weight	Abdomen circumference	Height	Spleen
7	Male	15.6 ± 1.8	23.7 ± 3.4	53.5 ± 4.1	123.7 ± 6.9	8.0 ± 0.8
	Female	13.6 ± 1.7	22.3 ± 3.7	54.3 ± 4.2	127.9 ± 3.5	7.9 ± 0.5
8	Male	15.7 ± 1.6	26.0 ± 3.7	54.3 ± 3.1	128.4 ± 5.7	7.5 ± 0.6
	Female	13.7 ± 2.3	22.1 ± 5.2	52.7 ± 6.8	126.8 ± 5.1	7.8 ± 0.5
9	Male	16.5 ± 1.6	29.5 ± 3.9	57.1 ± 4.9	133.7 ± 4.5	7.9 ± 0.7
	Female	19.6 ± 5.9	36.3 ± 11.8	63.3 ± 10.3	135.7 ± 4.1	9.9 ± 0.9
10	Male	16.7 ± 2.2	31.9 ± 4.3	58.7 ± 4.3	138.1 ± 5.8	8.6 ± 0.4
	Female	17.3 ± 3.3	34.2 ± 9.7	59.9 ± 8.1	140.0 ± 8.9	10.0 ± 0.3
11	Male	16.1 ± 2.2	32.3 ± 5.5	57.3 ± 4.5	141.3 ± 5.8	9.2 ± 0.7
	Female	17.3 ± 3.0	34.7 ± 6.4	60.4 ± 5.7	141.5 ± 4.6	9.5 ± 0.3
12	Male	18.3 ± 3.2	37.8 ± 8.3	57.8 ± 6.8	143.2 ± 4.4	9.7 ± 1.0
	Female	18.0 ± 2.7	39.8 ± 7.2	60.3 ± 6.8	148.6 ± 7.2	10.0 ± 0.3
13	Male	17.7 ± 2.4	40.3 ± 8.5	61.5 ± 7.0	150.3 ± 9.7	9.8 ± 0.7
	Female	20.2 ± 4.3	48.6 ± 10.3	66.1 ± 6.6	155.3 ± 7.5	10.5 ± 0.5

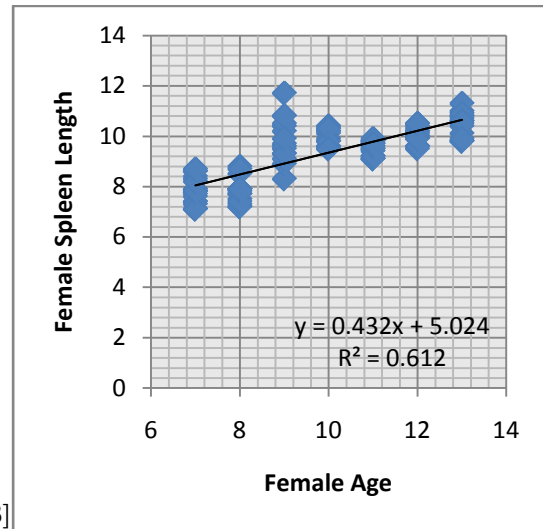
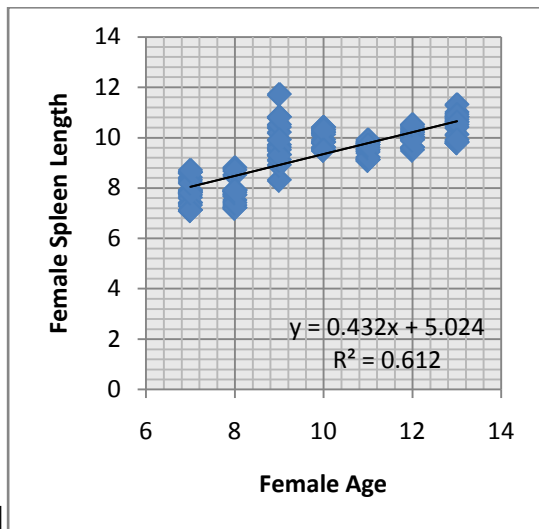
Values are expressed as Mean ± SD. *Body Mass Index (BMI)

Table 6 : Proximity Matrix of correlation between variables

	Correlations	BMI	Spleen	Weight	Abdomen circumference
BMI	Pearson Correlation	1.00	0.54	0.88	0.84
	P-value	.	0.000	0.000	0.000
Spleen	Pearson Correlation	0.54	1.00	0.71	0.55
	P-value	0.000	.	0.000	0.000
Weight	Pearson Correlation	0.88	0.71	1.00	0.85
	P-value	0.000	0.000	.	0.000
Abdomen circumference	Pearson Correlation	0.84	0.55	0.85	1.00
	P-value	0.000	0.000	0.000	.
Height	Pearson Correlation	0.43	0.72	0.79	0.56
	P-value	0.000	0.000	0.000	0.000

From above table (6) it was noticed that all p-values are less than 0.05 that means that there is relationship between the variables. The Pearson Correlation denotes values of the correlation either positive (+) or negative (-) as follows:

- 0.90 – 1.00 very strong relationship.
- 0.70 – 0.89 strong relationship.
- 0.50 – 0.69 middle relationship.
- 0.00 – 0.49 weak relationship



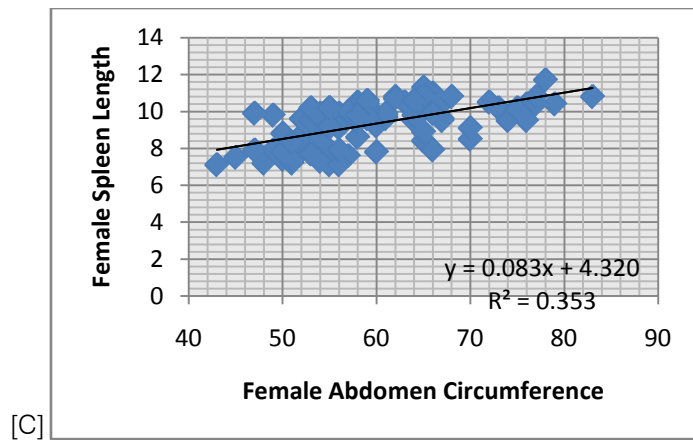


Figure 1 : [A,B,C] Scatter plot diagram shows the linear relationship between spleen length measured in (cm)and female BMI, age and abdomen circumference respectively

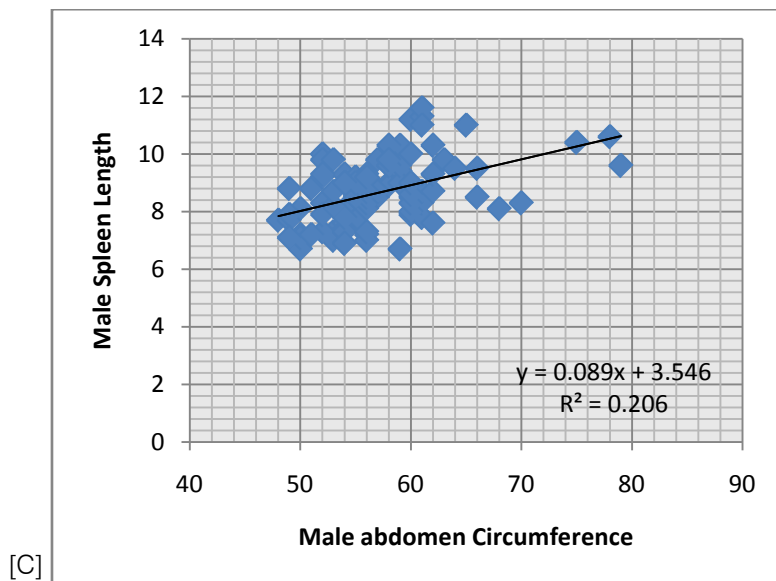
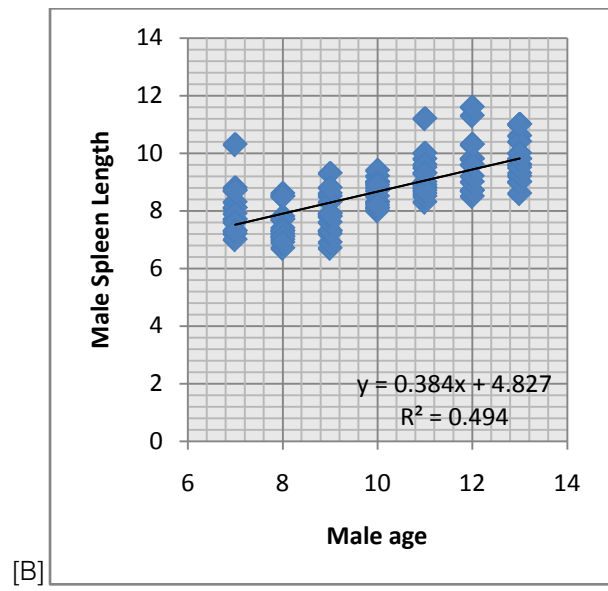
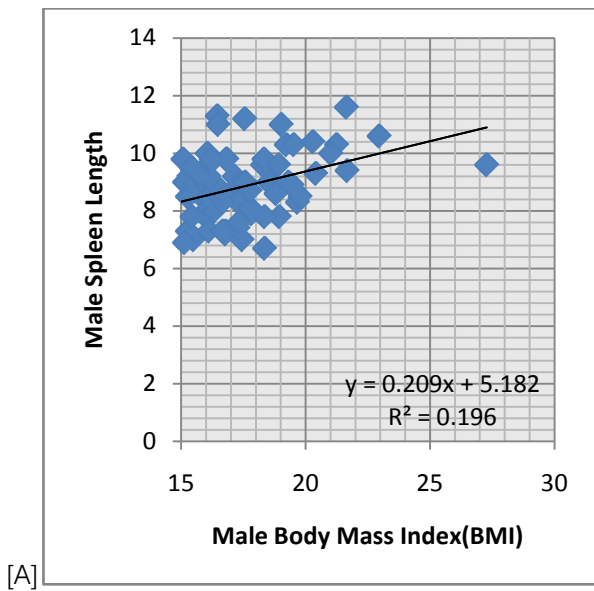


Figure 2 : [A,B,C] Scatter plot diagram shows the linear relationship between spleen length measured in (cm)and Male BMI, age and abdomen circumference respectively

IV. DISCUSSION

Ultrasound is simple and reliable in measuring the abdominal visceral organs without the risk of ionizing radiation. Measuring the volume is time-consuming and impractical in daily use and the longitudinal measuring of these organs is used as part of routine abdominal sonographic scanning for purposes of determining the normal anatomy [15]. Therefore, the longitudinal measurement was used because it is more practically considered.

The length of the spleen is an adequate indicator of size for most purposes and provides a useful baseline for monitoring changes in disease status. Establishing normal parameters is mandatory for defining the pathologic changes in size of the spleen, in routine sonographic examinations of children.[15]

This study included 104(48.4%) males, 111(51.6%) females of school children with ages from 7 up to 13. When measuring the spleen; 28 out of 215 (13.0%) got spleen length of 6.5-7.7 cm, 43(20%) of 5-8.4cm, 56(26%) of 8.5-9.4cm, 67(31.2%) of 9.5-10.4 and measurements greater than 10.5 were found in 21(9.8) of the sample. The mean spleen measurement was found to be 9.0 ± 1.2 (max 11.7, min 6.7), normal spleen has been investigated by only a few researchers [16]. When comparing our results with other similar results, we found that Sudanese children have less length than USA in all group of ages but greater than Greek [16], Indian [17] and Turkish populations [18]

When comparing the spleen length measurement with age in all group of ages it was found to be 7.9, 7.7, 8.9, 9.3, 9.4, 9.9, 10.1, 9.0 cm for the ages 7, 8, 9, 10, 11, 12, 13 respectively and the relation is significant between the spleen length and this group of children ages at p value 0.000.

DeLand [19] stated that the spleen showed variation according to sex and age. He reported that spleen in females was smaller than males in all age groups. But Niederau et al.[20] in their sonographic study, which was carried out on adults, found that spleen size decreased with increasing age.

In our study a significant difference was detected between males and females in spleen length and abdomen circumference measurements because P -value was found to be less than 0.05, that means the mean measurements values of spleen and abdomen circumference in females are greater than males and were found to be 9.3 ± 1.1 and 59.3 ± 8.1 , 8.7 ± 1.1 and 57.2 ± 5.6 respectively.

The study showed that the BMI, height, weight abdominal circumference have significant relation with the spleen length in all these group of ages.

From table (6) we noticed that all p -values are less than 0.05, that means there is a relationship between the variables. The Pearson Correlation denotes value of the correlation either positive (+) or negative (-)

as follows: 0.90 – 1.00 very strong relationship, 0.70 – 0.89 strong relationship, 0.50 – 0.69 middle relationship, 0.00 – 0.49 weak relationship.

Scatter plot diagrams showed the linear relationship between spleen length measured in (cm) and females and males, BMI, abdomen circumference (AC) and age respectively. The equations showed that the for BMI and AC, the spleen length was increased proportionally and by applying the following equations the spleen length can be estimated for these group of ages and known BMI and AC as :

For female Spleen length (cm) = $(0.432 \times \text{Age}) + 5.024$. For male Spleen length (cm) = $(0.384 \times \text{Age}) + 4.827$. For female Spleen length (cm) = $(0.172 \times \text{BMI}) + 6.368$, For male Spleen length (cm) = $(0.209 \times \text{BMI}) + 5.182$, For female Spleen length (cm) = $(0.083 \times \text{AC}) + 4.320$, For male Spleen length (cm) = $(0.089 \times \text{AC}) + 3.546$.

In conclusion, the spleen length obtained in this study was in different range of values reported in the previous studies. The mean spleen length in females is greater than males.

By applying the above equations the spleen length can be estimated. A local reference of spleen length was established; further studies are required to establish national reference of spleen length and volume in Sudan for both children and adults.

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- Shield the model - why did you employ this particular system or method? What is its compensation? You strength remark on its appropriateness from a abstract point of vision as well as point out sensible reasons for using it.
- Present a justification. Status your particular theory (es) or aim(s), and describe the logic that led you to choose them.
- Very for a short time explain the tentative propose and how it skilled the declared objectives.

Approach:

- Use past tense except for when referring to recognized facts. After all, the manuscript will be submitted after the entire job is done.
- Sort out your thoughts; manufacture one key point with every section. If you make the four points listed above, you will need a least of four paragraphs.



- Present surroundings information only as desirable in order hold up a situation. The reviewer does not desire to read the whole thing you know about a topic.
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- Do not take in frequently found.
- If use of a definite type of tools.
- Materials may be reported in a part section or else they may be recognized along with your measures.

Methods:

- Report the method (not particulars of each process that engaged the same methodology)
- Describe the method entirely
- To be succinct, present methods under headings dedicated to specific dealings or groups of measures
- Simplify - details how procedures were completed not how they were exclusively performed on a particular day.
- If well known procedures were used, account the procedure by name, possibly with reference, and that's all.

Approach:

- It is embarrassed or not possible to use vigorous voice when documenting methods with no using first person, which would focus the reviewer's interest on the researcher rather than the job. As a result when script up the methods most authors use third person passive voice.
- Use standard style in this and in every other part of the paper - avoid familiar lists, and use full sentences.

What to keep away from

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- Leave out information that is immaterial to a third party.

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The principle of a results segment is to present and demonstrate your conclusion. Create this part a entirely objective details of the outcome, and save all understanding for the discussion.

The page length of this segment is set by the sum and types of data to be reported. Carry on to be to the point, by means of statistics and tables, if suitable, to present consequences most efficiently. You must obviously differentiate material that would usually be incorporated in a study editorial from any unprocessed data or additional appendix matter that would not be available. In fact, such matter should not be submitted at all except requested by the instructor.



Content

- Sum up your conclusion in text and demonstrate them, if suitable, with figures and tables.
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- Present a background, such as by describing the question that was addressed by creation an exacting study.
- Explain results of control experiments and comprise remarks that are not accessible in a prescribed figure or table, if appropriate.
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Approach

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- Recommendations for detailed papers will offer supplementary suggestions.

Approach:

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<i>References</i>	Complete and correct format, well organized	Beside the point, Incomplete	Wrong format and structuring



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